

AMENDMENTS TO THE CLAIMS

1-4. (cancelled)

5. (currently amended) ~~The method of claim 4, A method for generating a simulated patient image, the method comprising:~~

- ~~_____ obtaining image data from an actual patient image;~~
- ~~_____ generating simulated noise data through a random number generator in accordance with a Poisson distribution;~~
- ~~_____ combining scan data from said actual patient image with said generated simulated noise data to create pre-image data;~~
- ~~_____ reconstructing said pre-image data to create simulated image data; and~~
- ~~_____ combining said simulated image data with said simulated noise data to create the simulated patient image;~~
- ~~_____ wherein individual scan data samples from said scan data are each combined with a random noise value generated from said Poisson distribution random number generator, said random noise value first being multiplied by a weighting factor to produce a weighted random noise value;~~

~~wherein-said weighting factor is-determined in accordance with the equation:~~

$$\alpha = \beta \sqrt{D \left(\frac{1}{\alpha} - 1 \right)} \quad ;$$

~~wherein α is said weighting factor, β is a scale factor whose value depends on a data acquisition system (DAS) gain and the image processing characteristics, α is a tube current reduction factor relative to a tube current at which said actual patient image was taken, and D is a DAS signal level for a corresponding individual scan data sample.~~

6. (original) The method of claim 5, wherein, in addition to said weighting factor, each of said random noise values are further multiplied by an electronic noise

scale factor prior to being combined with individual scan data samples, said electronic noise scale factor being determined in accordance with the equation:

$$\sigma_e = \alpha N_n P ;$$

wherein N_n is said electronic noise scale factor due to non-quantum noise, α is said weighting factor, P is said random noise value generated from said Poisson distribution random number generator, and σ_e is a standard deviation of said generated simulated noise data to be combined with said actual patient image.

7. (currently amended) ~~The method of claim 1, further comprising:~~ A method for generating a simulated patient image, the method comprising:

obtaining image data from an actual patient image;

generating simulated noise data by creating a set of individual noise pattern images for each of a plurality of phantom objects;

selecting at least one of said individual noise pattern images to be combined with said actual patient image; and

combining said at least one selected individual noise pattern image with said actual patient image, thereby creating the simulated patient image.

8. (original) The method of claim 7, wherein said selecting at least one of said individual noise pattern images is based upon a patient shape and an imaging technique.

9. (original) The method of claim 7, wherein said at least one of said individual noise pattern images is randomly selected.

10. (original) The method of claim 9, wherein if more than one of said individual noise pattern images is selected, then said noise pattern images are added together to produce a resultant noise pattern.

11. (original) The method of claim 10, wherein said combined noise pattern is scaled by a scaling factor, s , in accordance with the equation:

$$s = \frac{\sigma_n}{\sigma_p} \quad ; \text{ with}$$

$$\sigma_s = \sqrt{\sigma_f^2 - \sigma_o^2} = \sigma_o \sqrt{\left(\frac{1}{\alpha} - 1\right)}$$

wherein, σ_n is a standard deviation of said generated simulated noise data to be combined with said actual patient image, σ_p is a standard deviation of randomly selected interpolated and summed noise pattern images, σ_f is a desired standard deviation desired for the simulated patient image, σ_o is a standard deviation of said actual patient image and α is a tube current reduction factor relative to a tube current at which said actual patient image was taken.

12. (original) The method of claim 11, wherein said noise pattern images are scaled by the inverse square root of the number of said noise pattern images selected.

13. (original) A method for generating a simulated computer tomography (CT) patient image, the method comprising:

obtaining image data from an actual CT patient image taken at a first radiation dose;

generating simulated noise data; and

combining said image data with said simulated noise data to create the simulated patient image;

wherein the simulated image simulates said actual CT patient image taken at a second, reduced radiation dose with respect to said first radiation dose.

14. (original) The method of claim 13, further comprising:

combining scan data from said actual patient image with said generated simulated noise data to create pre-image data; and
reconstructing said pre-image data to create simulated image data.

15. (original) The method of claim 14 wherein said simulated noise data is generated through a random number generator in accordance with a Poisson distribution.

16. (original) The method of claim 15, wherein individual scan data samples from said scan data are each combined with a random noise value generated from said Poisson distribution random number generator, said random noise value first being multiplied by a weighting factor to produce a weighted random noise value.

17. (original) The method of claim 16, wherein said weighting factor is determined in accordance with the equation:

$$\alpha = \beta \sqrt{D \left(\frac{1}{\alpha} - 1 \right)} \quad ;$$

wherein α is said weighting factor, β is a scale factor whose value depends on a data acquisition system (DAS) gain and the image processing characteristics, α is a tube current reduction factor relative to a tube current corresponding to said first radiation dose, and D is a DAS signal level for a corresponding individual scan data sample.

18. (original) The method of claim 17, wherein, in addition to said weighting factor, each of said random noise values are further multiplied by an electronic noise scale factor prior to being combined with individual scan data samples, said electronic noise scale factor being determined in accordance with the equation:

$$\sigma_n = \alpha N_n P \quad ;$$

wherein N_n is said electronic noise scale factor due to non-quantum noise, α is said weighting factor, P is said random noise value generated from said Poisson

distribution random number generator, and σ_n is a standard deviation of said generated simulated noise data to be combined with said actual patient image.

19. (original) The method of claim 13, further comprising:

creating a set of individual noise pattern images for each a plurality of phantom objects;

selecting at least one of said individual noise pattern images to be combined with said actual patient image; and

combining said at least one selected individual noise pattern image with said actual patient image, thereby creating the simulated patient image.

20. (original) The method of claim 19, wherein said selecting at least one of said individual noise pattern images is based upon a patient shape and an imaging technique.

21. (original) The method of claim 20, wherein said at least one of said individual noise pattern images is randomly selected.

22. (original) The method of claim 21, wherein if more than one of said individual noise pattern images is selected, then said noise pattern images are added together to produce a resultant noise pattern.

23. (original) The method of claim 22, wherein said combined noise pattern is scaled by a scaling factor, s , in accordance with the equation:

$$s = \frac{\sigma_e}{\sigma_p} \quad ; \text{ with}$$

$$\sigma_s = \sqrt{\sigma_f^2 - \sigma_0^2} = \sigma_0 \sqrt{\left(\frac{1}{\alpha} - 1\right)}$$

wherein, σ_n is a standard deviation of said generated simulated noise data to be combined with said actual patient image, σ_p is a standard deviation of randomly selected interpolated and summed noise pattern images, σ_f is a desired standard deviation desired for the simulated patient image, σ_a is a standard deviation of said actual patient image and α is a tube current reduction factor relative to a tube current corresponding to said first radiation dose.

24. (original) The method of claim 23, wherein said noise pattern images are scaled by the inverse square root of the number of said noise pattern images selected.

25-28. (cancelled)

29. (currently amended) ~~The imaging system of claim 28,~~ An imaging system, comprising:

a gantry having an x-ray source and a radiation detector array, wherein said gantry defines a patient cavity and wherein said x-ray source and said radiation detector array are rotatably associated with said gantry so as to be separated by said patient cavity;

a patient support structure movably associated with said gantry so as to allow communication with said patient cavity; and

a processing device for obtaining image data from an actual patient image; means for generating simulated noise data through a random number generator in accordance with a Poisson distribution;

means for combining said image data with said simulated noise data to create a simulated patient image;

means for combining scan data from said actual patient image with said generated simulated noise data to create pre-image data; and

means for reconstructing said pre-image data to create simulated image data;

wherein individual scan data samples from said scan data are each combined with a random noise value generated from said Poisson distribution random number generator, said random noise value first being multiplied by a weighting factor to produce a weighted random noise value;

~~wherein~~ said weighting factor is determined in accordance with the equation:

$$a = \beta \sqrt{D \left(\frac{1}{\alpha} - 1 \right)} \quad ;$$

wherein a is said weighting factor, β is a scale factor whose value depends on a data acquisition system (DAS) gain and the image processing characteristics, α is a tube current reduction factor relative to a tube current at which said actual patient image was taken, and D is a DAS signal level for a corresponding individual scan data sample.

30. (original) The imaging system of claim 29, wherein, in addition to said weighting factor, each of said random noise values are further multiplied by an electronic noise scale factor prior to being combined with individual scan data samples, said electronic noise scale factor being determined in accordance with the equation:

$$\sigma_n = a N_n P \quad ;$$

wherein N_n is said electronic noise scale factor due to non-quantum noise, a is said weighting factor, P is said random noise value generated from said Poisson distribution random number generator, and σ_n is a standard deviation of said generated simulated noise data to be combined with said actual patient image.

31. (currently amended) ~~The imaging system of claim 25, further comprising:~~
An imaging system, comprising:

a gantry having an x-ray source and a radiation detector array, wherein said gantry defines a patient cavity and wherein said x-ray source and said radiation detector

array are rotatively associated with said gantry so as to be separated by said patient cavity;

a patient support structure movingly associated with said gantry so as to allow communication with said patient cavity; and

a processing device for obtaining image data from an actual patient image;

means for generating simulated noise data by

means for creating a set of individual noise pattern images for each of a plurality of phantom objects;

means for selecting at least one of said individual noise pattern images to be combined with said actual patient image; and

means for combining said at least one selected individual noise pattern image with said actual patient image, thereby creating the simulated patient image.

32. (original) The imaging system of claim 31, wherein said means for selecting at least one of said individual noise pattern images is based upon a patient shape and an imaging technique.

33. (original) The imaging system of claim 31, wherein said at least one of said individual noise pattern images is randomly selected.

34. (original) The imaging system of claim 33, wherein if more than one of said individual noise pattern images is selected, then said noise pattern images are added together to produce a resultant noise pattern.

35. (original) The imaging system of claim 34, wherein said combined noise pattern is scaled by a scaling factor, s , in accordance with the equation:

$$s = \frac{\sigma_a}{\sigma_p} \quad ; \text{ with}$$

$$\sigma_s = \sqrt{\sigma_f^2 - \sigma_o^2} = \sigma_o \sqrt{\left(\frac{1}{\alpha} - 1\right)}$$

wherein, σ_s is a standard deviation of said generated simulated noise data to be combined with said actual patient image, σ_p is a standard deviation of randomly selected interpolated and summed noise pattern images, σ_f is a desired standard deviation desired for the simulated patient image, σ_o is a standard deviation of said actual patient image and α is a tube current reduction factor relative to a tube current at which said actual patient image was taken.

36. (original) The imaging system of claim 35, wherein said noise pattern images are scaled by the inverse square root of the number of said noise pattern images selected.

37-40. (cancelled)

41. (currently amended) ~~The storage-medium of claim 40, A storage medium, comprising;~~

_____ a machine readable computer program code for generating a simulated patient image; and

_____ instructions for causing a computer to implement a method, the method further comprising;

_____ obtaining image data from an actual patient image;

_____ generating simulated noise data through a random number generator in accordance with a Poisson distribution;

_____ combining scan data from said actual patient image with said generated simulated noise data to create pre-image data;

_____ reconstructing said pre-image data to create simulated image data;

and

combining said simulated image data with said simulated noise data to create the simulated patient image;

wherein individual scan data samples from said scan data are each combined with a random noise value generated from said Poisson distribution random number generator, said random noise value first being multiplied by a weighting factor to produce a weighted random noise value;

wherein said weighting factor is determined in accordance with the equation:

$$\alpha = \beta \sqrt{D \left(\frac{1}{\alpha} - 1 \right)} \quad ;$$

wherein α is said weighting factor, β is a scale factor whose value depends on a data acquisition system (DAS) gain and the image processing characteristics, α is a tube current reduction factor relative to a tube current at which said actual patient image was taken, and D is a DAS signal level for a corresponding individual scan data sample.

42. (original) The storage medium of claim 41, wherein, in addition to said weighting factor, each of said random noise values are further multiplied by an electronic noise scale factor prior to being combined with individual scan data samples, said electronic noise scale factor being determined in accordance with the equation:

$$\sigma_a = \alpha N_n P \quad ;$$

wherein N_n is said electronic noise scale factor due to non-quantum noise, α is said weighting factor, P is said random noise value generated from said Poisson distribution random number generator, and σ_a is a standard deviation of said generated simulated noise data to be combined with said actual patient image.

43. (currently amended) ~~The storage medium of claim 37, further comprising:~~
A storage medium, comprising:

a machine readable computer program code for generating a simulated patient image; and

instructions for causing a computer to implement a method, the method further comprising;

obtaining image data from an actual patient image;

generating simulated noise data by creating a set of individual noise pattern images for each of a plurality of phantom objects;

selecting at least one of said individual noise pattern images to be combined with said actual patient image; and

combining said at least one selected individual noise pattern image with said actual patient image, thereby creating the simulated patient image.

44. (original) The storage medium of claim 43, wherein said selecting at least one of said individual noise pattern images is based upon a patient shape and an imaging technique.

45. (original) The storage medium of claim 43, wherein said at least one of said individual noise pattern images is randomly selected.

46. (original) The storage medium of claim 45, wherein if more than one of said individual noise pattern images is selected, then said noise pattern images are added together to produce a resultant noise pattern.

47. (original) The storage medium of claim 46, wherein said combined noise pattern is scaled by a scaling factor, s , in accordance with the equation:

$$s = \frac{\sigma_s}{\sigma_p} \quad ; \text{ with}$$

$$\sigma_s = \sqrt{\sigma_f^2 - \sigma_0^2} = \sigma_0 \sqrt{\left(\frac{1}{\alpha} - 1\right)}$$

wherein, σ_n is a standard deviation of said generated simulated noise data to be combined with said actual patient image, σ_p is a standard deviation of randomly selected interpolated and summed noise pattern images, σ_f is a desired standard deviation desired for the simulated patient image, σ_o is a standard deviation of said actual patient image and α is a tube current reduction factor relative to a tube current at which said actual patient image was taken.

48. (original) The storage medium of claim 47, wherein said noise pattern images are scaled by the inverse square root of the number of said noise pattern images selected.

49-52. (cancelled)

53. (currently amended) ~~The computer data signal of claim 52, A computer data signal, comprising:~~

~~_____ code configured to cause a processor to implement a method for generating a simulated patient image, the method further comprising:~~

~~_____ obtaining image data from an actual patient image;~~

~~_____ generating simulated noise data through a random number generator in accordance with a Poisson distribution;~~

~~_____ combining scan data from said actual patient image with said generated simulated noise data to create pre-image data;~~

~~_____ reconstructing said pre-image data to create simulated image data;~~

~~and~~

~~_____ combining said simulated image data with said simulated noise data to create the simulated patient image;~~

~~_____ wherein individual scan data samples from said scan data are each combined with a random noise value generated from said Poisson distribution random~~

number generator, said random noise value first being multiplied by a weighting factor to produce a weighted random noise value;

wherein said weighting factor is determined in accordance with the equation:

$$\alpha = \beta \sqrt{D \left(\frac{1}{\alpha} - 1 \right)} \quad ;$$

wherein α is said weighting factor, β is a scale factor whose value depends on a data acquisition system (DAS) gain and the image processing characteristics, α is a tube current reduction factor relative to a tube current at which said actual patient image was taken, and D is a DAS signal level for a corresponding individual scan data sample.

54. (original) The computer data signal of claim 53, wherein, in addition to said weighting factor, each of said random noise values are further multiplied by an electronic noise scale factor prior to being combined with individual scan data samples, said electronic noise scale factor being determined in accordance with the equation:

$$\sigma_n = a N_n P \quad ;$$

wherein N_n is said electronic noise scale factor due to non-quantum noise, a is said weighting factor, P is said random noise value generated from said Poisson distribution random number generator, and σ_n is a standard deviation of said generated simulated noise data to be combined with said actual patient image.

55. (currently amended) ~~The computer data signal of claim 49, further comprising:~~ A computer data signal, comprising:

code configured to cause a processor to implement a method for generating a simulated patient image, the method further comprising:

obtaining image data from an actual patient image;
generating simulated noise data by creating a set of individual noise pattern images for each a plurality of phantom objects;

selecting at least one of said individual noise pattern images to be combined with said actual patient image; and

combining said at least one selected individual noise pattern image with said actual patient image, thereby creating the simulated patient image.

56. (original) The computer data signal of claim 55, wherein said selecting at least one of said individual noise pattern images is based upon a patient shape and an imaging technique.

57. (original) The computer data signal of claim 55, wherein said selecting at least one of said individual noise pattern images is based upon a patient shape and an imaging technique.

58. (original) The computer data signal of claim 57, wherein if more than one of said individual noise pattern images is selected, then said noise pattern images are added together to produce a resultant noise pattern.

59. (original) The computer data signal of claim 58, wherein said combined noise pattern is scaled by a scaling factor, s , in accordance with the equation:

$$s = \frac{\sigma_a}{\sigma_p} \quad ; \text{ with}$$

$$\sigma_a = \sqrt{\sigma_f^2 - \sigma_0^2} = \sigma_0 \sqrt{\left(\frac{1}{\alpha} - 1\right)}$$

wherein, σ_a is a standard deviation of said generated simulated noise data to be combined with said actual patient image, σ_p is a standard deviation of randomly selected interpolated and summed noise pattern images, σ_f is a desired standard deviation desired for the simulated patient image, σ_0 is a standard deviation of said actual patient image

and α is a tube current reduction factor relative to a tube current at which said actual patient image was taken.

60. (currently amended) The computer data signal storage medium of claim 59, wherein said noise pattern images are scaled by the inverse square root of the number of said noise pattern images selected.